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Application of RPMI 2650 nasal cell model to a 3D printed apparatus for the testing of drug deposition and permeation of nasal products

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Title: Application of RPMI 2650 Nasal Cell Model to a 3D Printed Apparatus for the Testing of Drug Deposition and Permeation of Nasal Products

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Abstract: The aim of this study was to incorporate an optimized RPMI2650 nasal cell model into a 3D printed model of the nose to test deposition and permeation of drugs intended for use in the nose. The nasal cell model was optimized for barrier properties in terms of permeation marker and mucus production. RT-PCR was used to determine the xenobiotic transporter gene expression of RPMI 2650 cells in comparison with primary nasal cells. After 14 days in culture, the cells were shown to produce mucus, and to express trans-epithelial electrical resistance (TEER) values and sodium fluorescein permeability consistent with values reported for excised human nasal mucosa. In addition, good correlation was found between RPMI 2650 and primary nasal cells transporters expression values.

The purpose built 3D printed model of the nose takes the form of an expansion chamber with inserts for cells and an orifice for insertion of a spray drug delivery device. This model was validated against the FDA glass chamber with cascade impactors that is currently approved for studies of nasal products. No differences were found between the two apparatus.

The apparatus including the nasal cell model was used to test a commercial nasal product containing budesonide (Rhinocort, AstraZeneca, Australia). Drug deposition and transport studies on RPMI 2650 were successfully performed.

The new 3D printed apparatus that incorporate cells can be used as valid in vitro model to test nasal products in conditions that mimic the delivery from nasal devices in real life conditions.



UNIVERSITA' DEGLI STUDI DI PARMA

DIPARTIMENTO DI FARMACIA

Dear Professor Göpferich,

Please find attached a revised version of the manuscript "Application of RPMI 2650 Nasal Cell Model to a 3D Printed Apparatus for the Testing of Drug Deposition and Permeation of Nasal Products" (Ms. Ref. No EJPB-D-16-00441) taking into account all the suggestions from the reviewers.

The comments of the reviewers have been addressed and all the requested modification introduced in the revised text.

Please find here after a detailed list of the changes along with the relative comments by the two reviewers.

Kind regards,

Fabio Sonvico
Handwritten signature of Fabio Sonvico in black ink.

Answers to reviewers comments

Reviewer #1: The manuscript presented by Michele Pozzoli is very interesting, develops a novel method to determine the drug deposition, the transport studies of nasal formulations. Good correlation has been found between RPMI 2650 and primary nasal cells transporters expression values. Furthermore, the model proposed in the manuscript was validated against the FDA glass chamber with cascade impactors that is currently approved for studies of nasal products. I highly recommend the publication of this excellent work.

No modifications required.

Reviewer #4: Manuscript of Pozzoli et al. (EJPB-D-16-00441)

Pozzoli et al. developed a novel nasal model that allows assessment of deposition characteristics of nasal products as well as permeation behavior of the drugs using cultured cells. The model is very interesting; the experiments were planned and carried out carefully.

There are some points that should be addressed by the authors:

Major questions/comments:

1. Materials and methods, page 12, line 309: According to MIQE guidelines for qPCR analysis more than one housekeeping gene should be chosen. Also, it has to be verified that those genes are NOT influenced by the treatment in the chosen cells or cell line. Please comment why you did not follow this procedure and discuss this as a limitation of your study.

Ribosomal RNA, the central component of the ribosome is an abundant and one of the most conserved genes in all cells, as a consequence 18S rRNA was selected as reference gene as it is known to show less variance in expression across a wide variety of treatments when compared with other reference genes, such as ACTB and GAPDH. Recently, 18S rRNA has been indicated as the most suitable reference gene for qRT-PCR normalization of data from primary human bronchial epithelial cells infected by influenza A virus (Kuchipudi et al. Virology Journal 2012, 9:230).

In the experiments presented in this manuscript we compared gene expression for a range of human drug transporter genes between the cell line RPMI 2650 and primary nasal epithelial cells, with the aim to evidence their presence and eventual macroscopic differences.

Therefore, whilst we acknowledge that there are limitations to only using one reference gene in studies, we believe that this had no effect on the outcome or validity of the data presented in this manuscript.

A few lines justifying the choice of 18S rRNA have been added in Materials and Methods section. A statement about the limitation of this choice has been added in Results and Discussion.

2. Materials and methods, page 15, line 371 et seqq.: Did you analyze how many μg of the 96 μg spray dose were deposited on the cell inserts in the chamber? In this context please also specify what you used as the reference 100 % value to calculate percentage data in Figure 7 and Figure 8.

The amount of budesonide deposited on each cell insert was quantified as $0.79 \pm 0.25 \mu\text{g}$ (mean and standard deviation of 5 replicates as suggested in comment 4). For figure 7 and 8 the 100% was calculated as the total amount of drug recovered for each well i.e. the sum of budesonide transported through, found inside and remaining on the cell layer. This has been clarified in the text at page.

3. Materials and methods, page 15, line 382 et seqq.: Please describe aspects of your analytical method in more detail. What was your lower limit of quantification? Did you use an internal or external standard? Since you mention BDP being detected at 240 nm (line 388): was that your internal standard? When was the external standard added?

The method to detect budesonide was an already validated method reported in literature; the reference was added to the bibliography (Ref 29). Linearity of the method was assessed having as lower concentration 0.1 $\mu\text{g}/\text{ml}$, i.e. the LOQ of the published method.

The reference to BDP in the text was an unintended interpolation since it was not used as internal standard in the method and was never used in the experiments presented. The text has been amended.

4. Materials and methods, page 16, line 392 et seqq.: If I see it correctly there were never more than $n=3$ which representing the data population. Three replicates are alright when there is limited material. However, it is not clear why you did not perform more than three experiments, e.g. for the data represented in in Figure 7 and Figure 8, when it accounts for the major conclusions of your approach. For statistical analysis $n=3$ is not really sufficient, $n=5$ or 6 would be more convincing. If you only have $n=3$ then you have to ensure the normal distribution of the residuals before you compare values with a statistical test. Please comment and amend.

Additional experiments of deposition/transport were performed in order to increase the number of replicates to 5 (Figure 7 and Figure 8). This changed the mean amount of budesonide deposited on each cell insert ($0.79 \pm 0.25 \mu\text{g}$).

Minor questions/comments:

1. Introduction, page 3, line 81: The wording "these advantages" appears a bit odd after you discussed limitations and challenges in the preceding lines.

The text has been modified according to the suggestion.

2. Materials and methods, page 13, line 325: The printed nasal model you used is very interesting. Did you analyze the adsorption effects of budesonide to the

surface of the material? This might be a limitation of the model if strong adsorption occurs which might result in incomplete cleaning of the chamber. Please comment and discuss.

After the 3D printing process with ABS, the inner and outer surfaces of the modified chamber were treated with acetone to remove porosity, obtaining a smooth and impermeable surface. The validation process of the modified expansion chamber was aimed also to investigate the possibility of drug absorption on the plastic material. However, as showed in Table 3 no adsorption for budesonide was evidenced, as no differences in drug recovery was found between glass and plastic chamber.

3. Results and discussion, page 17, line 413 et seqq.: Please detail what you used as a qualification TEER value for your monolayers, i.e. a minimum TEER value to decide whether the monolayer was of sufficient quality for the experiments.

TEER values of $90 \Omega\text{cm}^2$ and above were considered good to perform experiments. This has been clarified in the text.

4. Results and discussion, page 22, line 547 et seqq.: Please detail whether budesonide has been identified as a substrate of one of the transporters that you identified.

In literature, budesonide has been shown to be substrate of P-glycoprotein (Ref 40: Inflamm Bowel Dis. 2004 Sep;10(5):578-83.). This information has been added to the text.

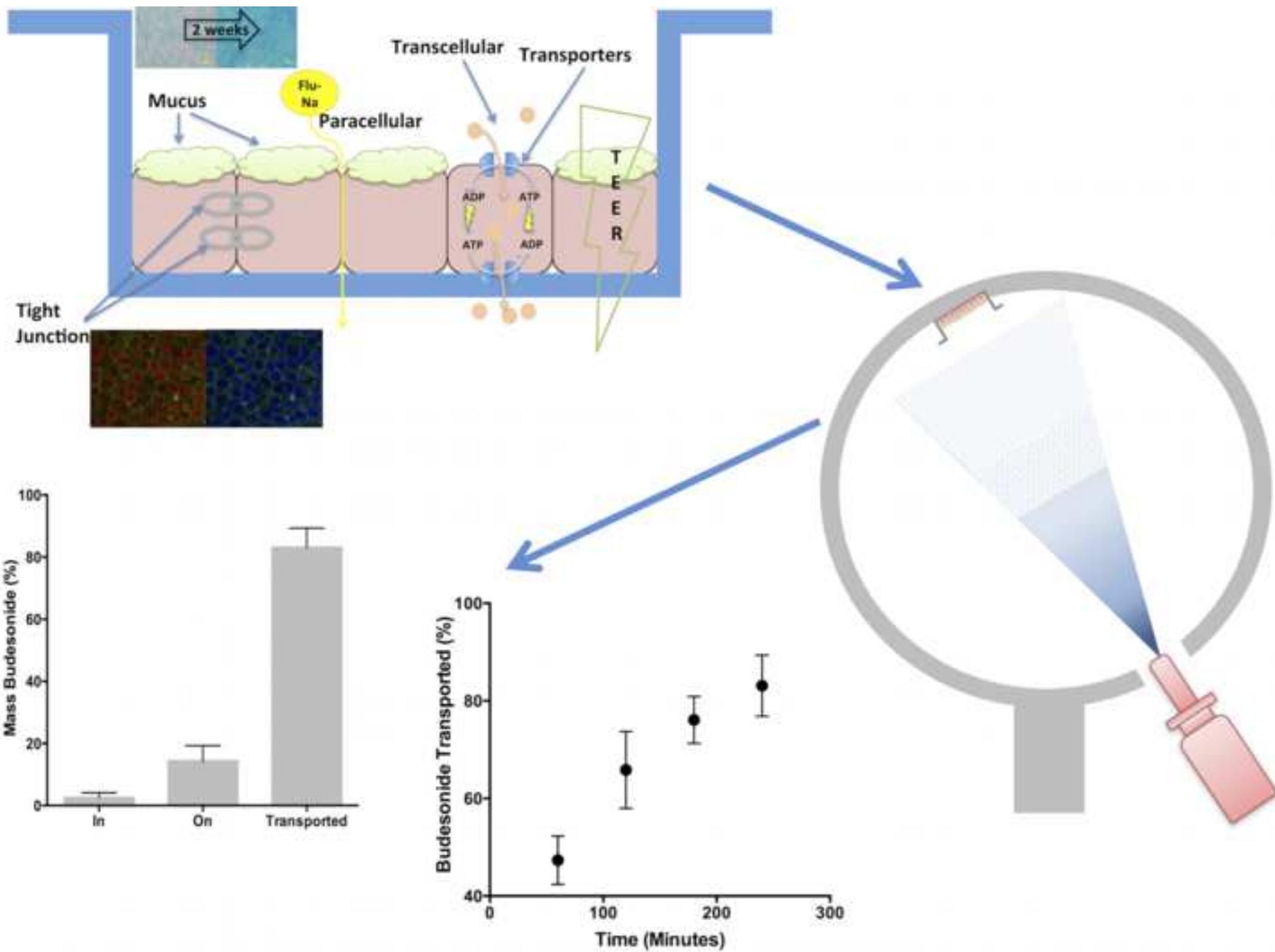
5. Results and discussion, page 28, line 684-686: This sentence appears to be odd with "showed" terminating the sentence.

The sentence has been modified.

Parma, 08/07/2016

Fabio Sonvico





1 **Application of RPMI 2650 Nasal Cell Model to a 3D Printed Apparatus for**
2 **the Testing of Drug Deposition and Permeation of Nasal Products**

3

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36 **Keywords:** RPMI 2650, Transporter Expression, Nasal Permeation, Mucus,
37 Air Liquid Interface, Primary Nasal Cell, 3D printing, Deposition, Dissolution,
38 Permeation

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43

44 **ABSTRACT**

45

46 The aim of this study was to incorporate an optimized RPMI2650 nasal cell
47 model into a 3D printed model of the nose to test deposition and permeation
48 of drugs intended for use in the nose. The nasal cell model was optimized for
49 barrier properties in terms of permeation marker and mucus production. RT-
50 qPCR was used to determine the xenobiotic transporter gene expression of
51 RPMI 2650 cells in comparison with primary nasal cells. After 14 days in
52 culture, the cells were shown to produce mucus, and to express TEER
53 (define) values and sodium fluorescein permeability consistent with values
54 reported for excised human nasal mucosa. In addition, good correlation was
55 found between RPMI 2650 and primary nasal cells transporters expression
56 values.

57 The purpose built 3D printed model of the nose takes the form of an
58 expansion chamber with inserts for cells and an orifice for insertion of a spray
59 drug delivery device. This model was validated against the FDA glass
60 chamber with cascade impactors that is currently approved for studies of
61 nasal products. No differences were found between the two apparatus.

62 The apparatus including the nasal cell model was used to test a commercial
63 nasal product containing budesonide (Rhinocort, AstraZeneca, Australia).
64 Drug deposition and transport studies on RPMI 2650 were successfully
65 performed.

66 The new 3D printed apparatus that incorporate cells can be used as valid *in*
67 *vitro* model to test nasal products in conditions that mimic the delivery from
68 nasal devices in real life conditions.

69 **INTRODUCTION**

70

71 Over recent decades, interest in the nose as an alternative site for drug
72 administration has increased steadily [1]. The nose is attractive for drug
73 delivery because the highly vascularised mucosa with low enzymatic activity
74 potentiates peptide permeation and rapid, high concentration drug absorption
75 that avoids first pass metabolism [2-6]. However, there are a number of
76 limitations and challenges associated with nasal drug delivery. Normal
77 mucociliary clearance would clear the nasal cavity of liquid formulations within
78 45 minute. The nasal cavity, even in health, is a small volume and
79 geometrically complex space, rendered smaller by mucosal inflammation.
80 Finally, the small volume of the cavity and the relatively low volume of fluid
81 available for drug dissolution limits the doses that can be administered [7-10].

82

83 Together, these **aspects** highlight the specificity of this administration route
84 and the need for further research into the development of new nasal
85 formulations that are able to overcome the challenges related to efficient
86 administration. In particular, there is an increasing need for reliable preclinical
87 tools to screen new products and formulations intended for nasal delivery that
88 can predict deposition and permeation through the mucosa and transport
89 across the epithelium.

90

91 Different *in vitro* models have been proposed to investigate the deposition of
92 nasal products. One approach is the use of transparent silicone anatomical
93 casts such as one originated from a Japanese male cadaver Koken (Koken
94 LM-005, Bunkyo-ku Tokyo, Japan). However, this as well as other casts,

95 appears to have some limitations related to the fact that the Food and Drug
96 Administration (FDA) do not regulate the deposition experiments, each cast is
97 not representative of the anatomical variability of different nasal cavities and
98 its polymeric surface is far from representative of the mucosal surface present
99 in the nose.

100

101 Another approach is to use Pharmacopoeia impactors, which have been used
102 to predict aerodynamic particle size distributions and thus deposition profiles
103 of aerosolized particles/droplets in the lower respiratory tract [11]. Specifically,
104 for nasal drug delivery, the FDA guidance for industry on “Bioavailability and
105 Bioequivalence Studies for Nasal Aerosols and Nasal Sprays for Local Action”
106 suggests to determine particles/droplets size distribution using a cascade
107 Impactor (CI) [12]. In particular, the guideline suggests the use of an induction
108 port, i.e. a glass expansion chamber (EC), to be connected to a cascade
109 impactor in order to maximise drug deposition below the top stages of the CI
110 [11-13]. This allows a better discrimination of particles with aerodynamic
111 diameters smaller than 10 μm that could be inhaled and therefore not suitable
112 for the nasal deposition.

113

114 While impactors and casts are important tools to determine deposition on the
115 different areas of the respiratory tract, they don't offer any information related
116 to either drug dissolution or permeation through the mucosa in the nasal
117 cavity. Recently, various approaches that integrate lower airway epithelia cell
118 cultures into compendia-based impactors have been proposed and used to
119 study the deposition and permeation of particles emitted by dry powder

120 inhalers and pressurized metered dose inhalers [14-16]. To our knowledge,
121 nothing similar has been proposed for nasal products as yet.

122

123 Among the *in vitro* cell lines available commercially, RPMI 2650 is the only
124 immortalized human nasal cell line. It has been studied as a drug permeation
125 tool by different researchers [2,17-22]. Initially, it was reported that this cell
126 line was unsuitable for permeation studies because it was not able to form a
127 confluent layer in conventional culture conditions [17]. However, Bai and
128 collaborators and, two years later, Wengst and Reichel, started to further
129 investigate culture condition for this cell line and to characterize some of the
130 culture features using transepithelial electrical resistance measurements
131 (TEER), permeation of paracellular markers and tight junctions' protein
132 expression. The key findings of these studies were that the change from the
133 conventional Liquid Cover Culture (LCC) to an Air Liquid Interface cultures
134 (ALI), where the upper surface of the cells was exposed to air, was able to
135 induce cell differentiation leading to the formation of cells layers suitable for
136 permeation experiments [18,19]. A few years later, Reichel and colleagues
137 tried to optimize culturing conditions using different cell growth media and
138 different types of cell-culture insert membrane; the main studies were based
139 on TEER observation and paracellular marker permeation. A pronounced
140 dependence of TEER on medium and membrane material were observed;
141 with the best culture condition being achieved when using polyethylene
142 terephthalate (PET) 3 μm porosity Transwell™ inserts, using Minimum
143 Essential Medium (MEM) supplemented with 10% of foetal bovine serum with
144 cells cultivated using the ALI condition [21].

145

146 Based on these previous findings, the aim of the present study is to
147 incorporate RPMI 2650 nasal cell epithelia, grown under ALI conditions into a
148 modified expansion chamber connected to a cascade impactor. This
149 approach, will allow the study of real nasal aerosols products, their deposition
150 and permeation after nasal device actuation. In order to develop this new
151 impactor/deposition apparatus, larger Snapwell™ cell culture inserts
152 detachable from its plastic frame that can be accommodated in to the 3D
153 apparatus without altering the aerosol performances of the impactor have
154 been selected [14]. Firstly, the optimization of the RPMI 2650 cell line culture
155 conditions on Snapwell inserts as nasal drug permeation model, specifically
156 focusing on parameters that characterize the barrier properties of the model,
157 i.e. TEER measurement, para-cellular marker permeation, tight junction
158 localization and mucus production, were investigated. To further validate the
159 model, a thorough analysis of the xenobiotic transporter expression in
160 comparison with that of freshly brushed human nasal cells was carried out.

161

162 Then, RPMI 2650 grown in ALI conditions on Snapwell inserts were
163 accommodated into a custom-built 3D printed modified expansion chamber in
164 order to study nasal product deposition and permeation after device actuation.
165 This new apparatus was validated against the original glass expansion
166 chamber, recommended in the FDA guidelines, in terms of drug deposition on
167 the CI stages and was tested in terms of drug deposition and permeation
168 through the RPMI 2650 nasal cell model, using a commercially available
169 budesonide nasal spray.

170 There is a clear need for a reliable preclinical model to test new products and
171 formulations intended for nasal delivery that can predict drug deposition,
172 permeation and transport across the epithelium.

173 **MATERIALS AND METHODS**

174

175 **Materials**

176 Minimum essential medium added with phenol red (MEM), non-essential
177 amino acids solution (×100), foetal bovine serum (FBS), L-glutamine (200
178 mM), Hank's balanced salt solution (HBSS), TrypLE Express, bovine serum
179 albumin (BSA) and phosphate buffered saline (PBS) were purchased from
180 Gibco, Invitrogen (Sydney, NSW, Australia). Snapwell™ cell culture inserts
181 (1.13 cm² polyester, 0.4 µm pore size) and black 96-well black plates were
182 supplied by Corning Costar (Lowell, MA, USA). All other culture plastics were
183 from Sarstedt (Adelaide, SA, Australia). Trypan blue solution (0.4%, w/v),
184 paraformaldehyde and dimethyl sulfoxide (DMSO) were obtained from Sigma-
185 Aldrich (Sydney, NSW, Australia). Fluorescein-sodium (Flu-Na) was
186 purchased from May & Baker Ltd. (Dagenham, England). Alcian blue 1% (pH
187 2.5) in 3% acetic acid was purchased from Fronine laboratory (Sydney, NSW,
188 Australia). NucleoSpin® RNA extraction kit was kindly provided by Scientifix
189 (Cheltenham, VIC, Australia), a custom TaqMan® Array-96 well plate and all
190 buffers were purchased by Applied Biosystem (ThermoFisher Scientific,
191 Scoresby, VIC, Australia). Rhinocort nasal spray (AstraZeneca, North Ryde,
192 NSW, Australia) was purchased at a local pharmacy. All chemicals and
193 reagents were of the highest analytical grade.

194

195 **Cell Culture Nasal Cell Line**

196 The cell line RPMI 2650 (CCL-30) was purchased from the American Type
197 Cell Culture Collection (ATCC, Manassas, VA, USA). Cells between passage
198 16-30 were grown in 75 cm² flasks in complete Minimum Essential Medium
199 (MEM) containing 10% (v/v) foetal bovine serum, 1% (v/v) non-essential
200 amino acid solution and 2mM L-glutamine and maintained in a humidified
201 atmosphere of 95% air 5% CO₂ at 37°C. Cells were propagated and sub-
202 cultured according to ATCC protocol. The cell culture inserts were coated with
203 250µl of 1µg/ml collagen solution in PBS (rat collagen type 1 in PBS, BD
204 Biosciences, Australia) and left overnight to increase the adherence of cells to
205 the membrane [18]. In order to establish the ALI model, 200 µl of cell
206 suspension were seeded on to the collagen coated Snapwell inserts at three
207 different seeding concentrations: 1.25, 2.5, 5.0 x10⁶ cells/ml (equivalent to
208 221, 442, 885 x10⁵ cells/cm²). The media on the apical compartment was
209 removed after 24 hours post-seeding. Media in the basolateral chamber was
210 replaced 3 times per week. Cell layers were allowed to grow and differentiate
211 under ALI conditions up to 21 days.

212

213 **Transepithelial electrical resistance Measurements**

214 Transepithelial electrical resistance was recorded with EVOM2[®] epithelial
215 voltohmmeter (World Precision Instruments, Sarasota, FL, USA) every 2-3
216 days from day one. Briefly, pre-warmed media was added to the apical
217 chamber and allowed to equilibrate for at least 30 minutes in a cell culture
218 incubator (humidified air with 5% CO₂ at 37°C). Blank filter values were

219 subtracted and TEER values were calculated normalizing the resistance
220 values with the Snapwell inserts area (1.13 cm²).

221

222 **Sodium Fluorescein Permeation Experiments**

223 Sodium Fluorescein, a paracellular marker (Flu-Na, MW 367 Da), was used to
224 evaluate barrier formation and tight junction functionality in the ALI culture.

225 Three time-points were chosen to conduct the experiments (1, 2, 3 weeks)

226 and at each time point, three Snapwell inserts were washed twice with warm

227 HBSS before each experiment. 250 µl of 2.5 mg/ml Flu-Na solution were

228 added to the apical chamber (donor) and 1.5 ml of pre-warmed HBSS into the

229 basolateral chamber (acceptor). At pre-determined time points, 200 µl of

230 solution are sampled from the acceptor chamber every 30 minutes over 4

231 hours and equal volume of fresh HBSS was added for replacement.

232 Samples were collected into a black 96-well plates and fluorescence of Flu-Na

233 was measured with a SpectraMax M2 plate reader (Molecular Devices,

234 Sunnyvale, CA, USA), using excitation and emission wavelengths of 485 nm

235 and 535 nm, respectively. The calibration coefficient of determination was

236 0.999, with standards prepared between 1.25 and 0.0125 µg/ml.

237 Samples were analysed and the permeation coefficient (P_{app}) was calculated

238 according Eq. (1):

$$P_{app} = \frac{dQ}{dt \cdot C_0 \cdot A}$$

239 Where dQ/dt is the flux (µg/s) of the Flu-Na across the barrier, C_0 is the initial

240 donor concentration (µg/ml) and A is the surface area (cm²).

241

242 **Evaluation of Mucus Production**

243 To assess the ability of the cell line RPMI 2650 to produce mucus when
244 cultured at the ALI configuration, Alcian Blue was used according to a
245 previously established method [23]. Mucus production of the ALI model was
246 assessed at different time points (1, 7, 14, 21 days) for three seeding
247 densities (1.25 , 2.5 , 5.0×10^6 cells/ml), respectively. On the day of the
248 experiment, cell layers were washed twice with $300 \mu\text{l}$ of pre-warmed PBS
249 and fixed using 4% (w/v) paraformaldehyde for 20 minutes. After the fixing
250 agent was washed with PBS, the surface of the cells was stained with Alcian
251 Blue. Excess staining was washed with PBS and inserts allowed to air-dried
252 for approximately three hours. The membrane was cut from the insert and
253 mounted on to the glass slide with Entellan™ mounting medium (ProSciTech,
254 Thuringowa, QLD, Australia) and sealed. Subsequently, images were taken
255 using an Olympus BX60 (Olympus, Hamburg, Germany) microscope
256 equipped with an Olympus DP71 camera. Three images were taken per well,
257 with all conditions performed in triplicate. Images were analysed using Image
258 J software (NIH, Bethesda, MD, USA) and values of RGB (Red Green Blue)
259 were measured for each image [24]. The ratio of blue (RGBb ratio) was
260 calculated by dividing the mean RGBb by the sum of the RGB values for each
261 image (R_GB_r + R_GB_g + R_GB_b) [23].

262

263 **Immunocytochemistry Experiment**

264 In order to visualise the tight junction proteins on RPMI 2650 cells: ZO-1
265 (zone occluding 1) and E-cadherin immunocytochemistry was performed.
266 RPMI 2650 cells grown on Snapwell inserts for 14 days under ALI condition

267 were used for immunocytochemistry. The cells were washed 3 times for 30
268 min with PBS to decrease the amount of mucus on the cell layers and
269 improve visualisation. Then, the cells were fixed with 4% paraformaldehyde
270 solution for 10 min. Afterwards, the cells were incubated for 10 min in PBS
271 containing 50 mM NH₄Cl, followed by 8 min with 0.1% (w/v) Triton X-100 in
272 PBS for permeabilization of the cell membrane.

273

274 Cells were then incubated for 60 min with primary antibodies, i.e. 200 µL of E-
275 cadherin (H-108) rabbit polyclonal IgG (1:100, Santa Cruz Biotechnology,
276 Dallas, TX, USA) and ZO-1 (D7D12) rabbit monoclonal IgG (1:1000, Cell
277 Signaling Technology, Danvers, MA, USA). Afterwards, cell monolayers were
278 rinsed three times with PBS containing BSA 2%, before 30 minutes incubation
279 with 200 µL of a 1:500 dilution in PBS containing 2% BSA of a goat anti-
280 Rabbit IgG secondary antibody labelled with Alexa Fluor[®] 488
281 (LifeTechnologies, Waltham, MA, USA). 4',6-diamidino-2-phenylindole (DAPI,
282 1 µg/ml in PBS) was used to counterstain cell nuclei. After 30 min of
283 incubation, the specimens were again rinsed three times with PBS containing
284 2% BSA and embedded in Entellan[™] new mounting medium (Merk-Millipore,
285 Darmstadt, Germany). Images were obtained using a confocal laser-scanning
286 microscope (Nikon A1, Nikon Instruments Inc., Melville, NY, USA), using a
287 laser at 488 nm and 60x objective.

288

289 **Expression of Xenobiotic Transporters**

290 *RPMI 2650 Cell Culture and Sample Collection of Primary Nasal Cell*

291 RPMI 2650 cells were cultured for 14 days on Snapwell porous membranes
292 under ALI conditions at a density of 2.5×10^6 cells/ml. To obtain primary nasal
293 cells, bilateral nasal mucosal brushing was performed using a disposable
294 cytology brush (Model BC-202D-2010, Olympus Australia Pty. Ltd., Notting
295 Hill, VIC, Australia) on human subjects to collect nasal epithelium as
296 described previously [25-28]. Samples were pooled together from eight
297 healthy volunteers between ages 20 and 40, with two groups of four people
298 per gender. Samples were washed and centrifuged twice with PBS solution
299 and left in -80°C freezer overnight prior to RNA extraction.

300

301 *RNA Isolation, Target Synthesis, Microarray Data Analysis*

302 In order to analyse the protein transporter expression in the cells samples,
303 RNA was isolated and purified using the NucleoSpin[®] RNA kit (Machery-
304 Nagel, Düren, Germany). The RNA samples were treated with RNase-free
305 DNase sets and dissolved in RNase-free water. Concentration and purity was
306 determined by spectrophotometry (NanoDrop 2000, ThermoFischer Scientific,
307 Scoresby, VIC, Australia). TaqMan[®] Array Plates (LifeTechnologies, Sydney,
308 NSW, Australia) was used to perform RT-qPCR assays. The array, *ad hoc*
309 designed, enabled the assessment of 46 human drug transporter genes,
310 including 13 ATP-binding cassette transporters, 23 solute carrier transporters,
311 and 10 solute carrier organic anion transporters (see Table 1 for a list of all
312 genes and proteins). Reverse transcription was carried out using a
313 standardized internal protocol. Briefly, to 5 μl of RNA were added a mixture of
314 general primer and deoxynucleotide (dNTP, 1:1) and 5 μl of PCR grade water;
315 the mixture was heat at 65°C for 5 min and quickly cooled in ice.

316 Subsequently, 4 μ l of first strand buffer, 2 μ l of 0.1 M solution of DTT
317 (Dithiothreitol) and 1 μ l of ribonuclease inhibitor were added; the solution was
318 incubated at 37°C for 2 minutes and 1 μ l of M-MLV (Moloney Murine
319 Leukemia Virus) reverse transcriptase was added. The mixture was incubated
320 firstly at 25°C for 10 minutes and then at 37°C for 50 minutes; in order to stop
321 the reaction the temperature was raised to 70°C for 15 min. The cDNA for all
322 the samples was uniformly diluted to 20 ng/ μ l and mixed with TaqMan[®]
323 mastermix. Thermal-cycling conditions were set to manufacturer
324 specifications, with 20 μ l of mixture (sample and mastermix 1:1) were added
325 to each well. The plates were analysed using the StepOnePlus™ Real-Time
326 PCR System (Applied biosystem, ThermoFisher Scientific, Scoresby, VIC,
327 Australia) for a total of 40 cycles. Data analysis was performed using the Δ Cq
328 method, where the Δ Cq value is normalized to the 18S ribosomal RNA (18S
329 rRNA) used as a reference gene. Ribosomal RNA, the central component of
330 the ribosome is an abundant and one of the most conserved genes in all cells.
331 Recently, 18S rRNA has been indicated as the most suitable reference gene
332 for qRT-PCR normalization of data from primary human bronchial epithelial
333 cells [29].

334

335

336 **Development and Validation of Aerosol Nasal Deposition Apparatus**

337 *Development of the Modified Expansion Chamber*

338 Rapid prototyping with 3D printing technique was used to manufacture the
339 custom-made modified expansion chamber (MC) (Figure 1). The MC was
340 designed to accommodate up to 3 Snapwell cell culture inserts, using CAD

341 software (Catia 3D, 3DS, Boston, MA, USA). The modified expansion
342 chamber was designed based on the 2L glass expansion chamber (EC) as
343 suggested in the FDA guidance for nasal products [12]. The MC comprises of
344 two interlocking hemispheres: the lower part presents the connection to the
345 cascade impactors (through a connection adaptor), and an inlet hole for nasal
346 devices at 30° from the axis. The upper half is designed to allow the
347 incorporation of three Snapwell cell culture inserts, located opposite to the
348 inlet hole (Figure 1).

349

350 Acrylonitrile butadiene styrene (ABS) was used as printing material using a
351 commercial 3D printer (Dimension Elite, StrataSys, Eden Praire, MN, USA), at
352 layer thickness of 178 µm. Due to the intrinsic porosity of the printed material,
353 the internal and external surfaces were chemically treated with small
354 quantities of acetone to seal internal surfaces; absence of leakage was
355 successfully tested with different mixtures of water and methanol.

356

357 (Figure 1 Here)

358

359 *Validation of the Impactor Deposition Performances: Standard vs. Modified*
360 *Expansion Chamber*

361 Rhinocort, a commercial available nasal spray for the treatment of rhinitis
362 (AstraZeneca, North Ryde, NSW, Australia), containing a suspension of
363 Budesonide (32 µg/spray) as active ingredient, was used to validate the
364 modified chamber. Aerodynamic particle size distributions were evaluated
365 using a British Pharmacopoeia Apparatus E – Next Generation Impactor

366 (Westech W7; Westech Scientific Instruments, Upper Stondon, UK) (Figure
367 2). Analyses were performed in triplicate with either the glass expansion
368 chamber or the modified chamber fitted with Snapwell inserts. The device was
369 primed to waste and for each analysis, three actuations were fired. Briefly, the
370 impactor was connected to a rotary pump (Westech Scientific Instruments,
371 Upper Stondon, UK) at a flow-rate of 15 L/min using a calibrated flow meter
372 (Model 4040, TSI Precision Measurement Instruments, Aachen, Germany).
373 Each impactor stage was washed with a solution 80:20 (% v/v)
374 methanol/water and samples analysed by high performance liquid
375 chromatography (HPLC) using a validated method [30].

376

377 (Figure 2 Here)

378

379 *Validation of the Cell Layer Integrity in the Modified Chamber*

380 RPMI 2650 were cultivated on Snapwells at the optimized seeding condition.
381 At day 14, three cell inserts were washed with pre-warmed HBSS, and placed
382 into the modified expansion chamber. An HBSS solution into a VP3 Aptar
383 nasal pump (Aptar, Le Vaudreuil, France) was used as blank to simulate the
384 deposition process into the modified chamber. After 6 actuations of the buffer
385 blank solution, with the same deposition method previously described, the
386 inserts were transferred into a cell culture plate. Flu-Na permeation studies
387 were performed as mentioned above in order to confirm that the integrity of
388 the cell layers after aerosol deposition. The P_{app} was compared with untreated
389 control cells.

390

391 **Deposition and Transport of a Commercial Budesonide Nasal Spray on**
392 **Optimized RPMI 2650 cell Model using the Modified Expansion Chamber**

393 RPMI 2650 cells were used after 14 days from seeding on Snapwells (2.5
394 $\times 10^6$ cells/ml). Three cell inserts were washed with pre-warmed HBSS buffer
395 and fitted into the upper hemisphere of the modified expansion chamber. The
396 aerosol deposition of budesonide on the cell surface from the Rhinocort
397 device (AstraZeneca, North Ryde, NSW, Australia) was obtained according
398 method described above, with a total dose of 96 μg of budesonide (3 sprays)
399 was delivered into the chamber. The cell inserts were then removed from the
400 modified chamber and transferred to a 6-well plate containing 1.5 ml of fresh
401 pre-warmed HBBS. Samples of 200 μl were collected from the basal chamber
402 every hour and replaced with the same volume of fresh buffer. After four
403 hours, the apical surface of the epithelia was washed twice in order to collect
404 any remaining drug. Subsequently, cells were scraped from the insert
405 membrane and lysed with CelLytic™ buffer (Invitrogen, Sydney, NSW,
406 Australia) in order to quantify the amount of budesonide inside the cells by
407 HPLC. TEER measurements were performed prior and after the deposition in
408 order to confirm that the integrity of the cell layer was maintained.

409

410 **Analytical Quantification of Budesonide**

411
412 The amount of budesonide in each sample was determined using an HPLC
413 system equipped with a SPD-20A UV-Vis detector (Shimadzu, Tokyo, Japan)
414 according to a validated method reported in literature [30]. Briefly, a Luna C18
415 column (150 X 4.6 mm, 3 μm , Phenomenex, Lane Cove, NSW, Australia) was
416 used with a mobile phase methanol/water 80:20 % v/v. The flow rate was set

417 at 1 ml/min and **budesonide** was detected at $\lambda=240$ nm. The retention time of
418 budesonide was around 5 minutes. Standards were prepared in the mobile
419 phase, and 100 μ l injections were used. Linearity was confirmed between 0.1
420 μ g/ml and 50 μ g/ml [30].

421

422 **Statistics**

423 Unless differently stated, data represent the mean \pm standard deviation of at
424 least three independent experiments. t-Test was used to compare data, with
425 differences considered significant for $p < 0.05$.

426

427

1 **RESULT AND DISCUSSION**

2

3 **Transepithelial Electrical Resistance (TEER) Measurements**

4 Transepithelial electrical resistance can be used as an indicator of the development
5 and integrity of the epithelial barrier. Various studies have tried to optimize and
6 standardize the culture conditions of RPMI 2650 [21, 22]. However, the effects of
7 seeding density on RPMI 2650 cultured in the ALI conditions on this Snapwell insert
8 with a larger surface area has not been previously evaluated. The Snapwell inserts
9 offers a more flexible membrane compared to the more common 0.33 cm² Transwell
10 inserts due to their larger surface area and different support structure.

11

12 (Figure 3 Here)

13

14 The progressive formation of the tight junction barrier by cultured RPMI 2650 cells
15 seeded onto Snapwell inserts with respect to time is shown in Figure 3. The TEER
16 for the three different seeding densities steadily increases with time until day 14,
17 starting from values around 20 $\Omega\cdot\text{cm}^2$ and reaching a plateau between 115 $\Omega\cdot\text{cm}^2$
18 (5×10^6 cells/ml seeding) and 150 (1.25×10^6 cell/ml seeding) up to day 17 when the
19 TEER starts to decrease. Data indicate that at least 14 days are required for the cell
20 to reach a tight confluent layer with the highest TEER barrier when cultured in the
21 ALI conditions. After 17 days, a decrease of the TEER values is observed,
22 suggesting that the cells either start to die or lose their tight junction integrity a few
23 days after full maturation. This trend is similar to previously published data [21].
24 Regarding the three different seeding levels, no statistical differences were found at

1 | days 14 and 17, reaching values around 90-150 $\Omega\cdot\text{cm}^2$. Therefore, values above 90
2 | $\Omega\cdot\text{cm}^2$ were considered sufficient to perform experiments.

3
4 | We report a clear correlation with the range of TEER values reported for human
5 | nasal mucosa. our results are very similar to those reported previously [18,21,31]. In
6 | particular, TEER values from excised human mucosa obtained from turbinectomy
7 | surgeries and used within an hour from the extraction, showed TEER values around
8 | 90-180 $\Omega\cdot\text{cm}^2$. Therefore, this data support the use of ALI cultured RPMI 2650 as a
9 | representative model of the nasal mucosa.

11 | **Sodium Fluorescein Permeation Experiments**

12 | The relatively high variability in TEER values reported in literature for RPMI 2650
13 | cells suggests that this measurement is affected by many factors related to the
14 | technique (inter/intra laboratory), therefore other parameters have to be considered
15 | when trying to establish a model for drug deposition and transport. Thus, permeation
16 | studies of Flu-Na were performed in order to confirm and support the TEER
17 | measurements. Sodium fluorescein, due to its hydrophilic characteristic, is used as a
18 | paracellular permeation marker. The transport of Flu-Na across RPMI 2650 cell layer
19 | was evaluated over a period of 4 hours (Table 2). In order to confirm that, the
20 | Snapwell insert membrane were not the rate-limiting step of the permeation process,
21 | permeability of Flu-Na through the Snapwells membrane alone was also tested and
22 | showed a significantly higher value (1.38×10^{-5} cm/s).

23
24 | (Table 2 Here)

1 As shown in Table 2, no statistical difference was observed between the P_{app} values
2 of the three different seeding densities after a week of culture, suggesting that seven
3 days in ALI conditions are not sufficient to have a tight confluent cell layer. After 14
4 day of culture, the P_{app} values significantly decreased, when compared to the values
5 of week 1, supporting the findings of the TEER experiments. It was also found that
6 the intermediate seeding density reaches the lowest value of $2.68 \pm 0.60 \times 10^{-6}$ cm/s
7 after two weeks in culture. On the other hand, the lowest seeding density (1.25×10^6
8 cells/ml) shows higher permeability compared to the others two, suggesting that the
9 amount of cell may not sufficient to guarantee enough barrier properties. No
10 significant differences between the P_{app} values for the two higher seeding densities
11 were observed. After three weeks in culture, no significant difference in the Flu-Na
12 permeability was found for any of the seeding densities, suggesting two weeks in
13 culture is enough to reach a mature model with confluent cells for RPMI 2650.

14

15 Different research groups have tried to characterize the paracellular permeability of
16 RPMI 2650 grown in ALI conditions: Bai et al obtained values of 5.07×10^{-6} using
17 mannitol as marker [19]; Wengst and Reichel, using Flu-Na, on cells grown on
18 Transwell[®] polycarbonate membrane, presented values of 6.09×10^{-6} cm/s [18]; and
19 Reichel obtained lower values of 1.91×10^{-6} cm/s using Thincert[®] inserts with
20 polyethylene terephthalate membranes, confirming that the supporting material may
21 affect the adhesion and the layer/barrier formation of RPMI 2650 cell line [18,21].
22 More recently, Kreft reported P_{app} values of 6.08×10^{-7} cm/s using dextran conjugated
23 to fluorescein isothiocyanate (MW 10,000), an extremely low value that is related to
24 the higher molecular weight of the molecule used for the investigation [20].

25

1 **Evaluation of Mucus Production**

2 Mucus plays an important role in protecting the nasal epithelium. Furthermore, this
3 mucus is the first barrier that any drug administered into the nose has to overcome in
4 order to be absorbed; it has a key role also in the dissolution process of drug that will
5 allow subsequent permeation [32]. Thus, an appropriate model of the nasal
6 epithelium requires mucus of specific depth, biochemistry and rheology. Therefore,
7 the production of mucus in the RPMI 2650 cellular model grown in ALI condition was
8 investigated.

9

10 Alcian Blue allows mucus detection by reaction with acidic polysaccharides
11 (mucopolysaccharides) and sialic acid containing glycoproteins, producing a blue
12 color. Figure 4 shows an example of the staining of the mucus layer of RPMI2650
13 seeded at 2.50×10^6 cell/ml over a 3 week period.

14

15 (Figure 4 Here)

16

17 Observing the images in Figure 4 it can be seen that, after one day of culture, just
18 few light blue spots appear, most probably due to the staining of the extracellular
19 matrix. After one week of culture the cell layer is almost completely covered by a thin
20 but discontinuous light blue layer, but the increased blue intensity implies that a
21 small amount of mucus has been produced. At 14 days, the higher intensity of the
22 colour and its uniformity suggest that the production of mucus has increased and
23 that a mucus blanket uniformly covers the cell layer. At day 21, the mucus still cover
24 all the area but not uniformly, dark blue areas are alternate to light ones; this could

1 be related to the concurrent decrease in TEER between day 14-21 suggesting cell
2 integrity and/or death occurs.

3

4 The relative quantification of the mucus production was measured by the RGBb
5 ratio. Figure 5 shows the mucus production in terms of RGBb ratio over three weeks.
6 No differences in mucus production can be observed between the different seeding
7 densities at day 1 and day 7. However, at week 2, the intermediate (2.50×10^6
8 cell/ml) seeding shows a statistically significant increase in mucus production that
9 was statistically higher than the other two densities. This RGBb value subsequently
10 plateaus from day 14 to day 21. While the lowest and highest seeding densities (1.25
11 and 5.0×10^6 cell/ml) showed no statistically differences at both day 14 and 21.
12 These two seeding conditions showed a steady increase in the RGBb ratio value
13 indicating a build-up in the mucus production during all the culturing time. Finally at
14 day 21, all three seeding density managed to attain similar amount of mucus
15 produced with no significant differences observed between them.

16

17 These results suggest that the intermediate seeding density (2.50×10^6 cell/ml) is the
18 optimum condition that allows the cells to form confluent layer with a uniform mucus
19 blanket in 2 weeks in the Snapwell insert. This is probably due to the optimisation of
20 the growth conditions that allow for the cells to proliferate, sufficient nutrients and
21 space to interact and form tight junctions and produce mucus.

22

23 The plateau observed for the intermediate seeding density, can also be a result of
24 the limitations of measurement technique leading to a saturation of the blue RGBb
25 ratio [23]. In addition, being an *in vitro* model, one of the limitations is the static

1 nature of this system where the mucus cannot be cleared leading to build up in the
2 wells with the increasing cell numbers.

3

4 Based on the above results for mucus production, TEER measurements and Flu-Na
5 permeability, the optimal seeding density was found to be 2.50×10^6 cell/ml for RPMI
6 2650 cells grown on Snapwell inserts.

7

(Figure 5 Here)

8

9

10

1 **Immunocytochemical investigation**

2 Tight junctions play an important role in the control of the paracellular permeation
3 across the epithelia [33]. In order to confirm that the RPMI 2650 cells on Snapwell
4 inserts were also able to produce tight junctions, the expression and localization of
5 two proteins essential for the formation and maintenance of tight junction were
6 investigated; specifically, E-cadherin and *zonula occludens* protein 1 (ZO-1) (Figure
7 6). Figure 6A shows the localization of E-cadherin (green) around the nucleus
8 stained with DAPI (blue) and Figures 6B and C show in green the expression of ZO-
9 1 and in red DAPI.

10

11 As expected, the proteins are found at the edge of the cells where they are involved
12 in the formation of tight junction in the RPMI 2650 cells. Furthermore, the RPMI 2650
13 cells was found to form multilayers as seen with the overlapping nuclei in Figure 6C.
14 This is different from what Bai et al as observed, where cells were forming a
15 monolayer. However it is in good agreement with Kreft et al that noticed a multi-
16 layering growth of RPMI 2650 when cultured in ALI conditions [19,20].

17

18 (Figure 6 Here)

19

20 **Expression of Xenobiotic Transporters**

21 When paracellular transport across epithelia is not involved, membrane carrier
22 proteins can have a key role in the absorption, distribution and elimination processes
23 of both endogenous compounds and xenobiotics [34,35]. In order to cross the
24 epithelia a molecule needs to pass through two barriers; specifically it needs to be

1 taken up from apical membrane and effluxed from the basal membrane. These
2 processes are often carrier mediated [36].

3

4 In order to evaluate if RPMI 2650 could be a representative model of the nasal
5 mucosa, further investigation on the transporters expression in the cell line model
6 was performed and was compared with freshly brushed human nasal cells.

7

8 Specifically, 47 xenobiotic transporters were investigated. The genes investigated
9 were those expressing ATP Binding Cassette (ABC), Solute Carrier (SLC) and
10 Solute Carrier Organic anion (SLCO) proteins. Table 1 graphically summarizes
11 which of these 47 xenobiotic transporters were present in the RPMI 2650 cells and
12 compared with gene present on PNC: human primary nasal cells from brushing
13 (average between male and female).

14

(Table 1 Here)

15

16
17 For the RPMI 2650 cells, the highly expressed genes ($\Delta Cq < 5$) were found to be
18 MRP1 and MRP9 proteins while the poorly expressed genes ($\Delta Cq > 15$) were found
19 to be for the following transporters: BSEP (Bile Salt Export Pump), MRP5 (Multidrug
20 Resistance-associated Protein 5), MRP7, MRP8, OCT3 (Organic Cation Transporter
21 3), CNT3 (Anti-Concentrative Nucleoside Transporter 3), ENT1 (Equilibrative
22 nucleoside transporter 1) and ENT3. Some genes, such as those expressing MRP6,
23 PEPT1 (Peptide transporter 1), PEPT2, NaPi1 (Renal type I sodium/phosphate
24 transporter), OCT1, OCT2, URAT1 (Organic anion/urate transporter 1), ATB(0+)
25 (Sodium- and chloride-dependent neutral and basic amino acid transporter B(0+)),
26 OATP-C (Organic anion transporter polypeptide C), OATP-8, OATP-F, OATP-B were

1 not expressed at all. All the other genes were expressed at an intermediate level
2 ($5 < \Delta Cq < 15$).

3 In terms of the primary nasal cells obtained by nasal mucosa brushing, no
4 differences were found between male and female volunteers. Highly expressed
5 genes were those encoding for the following transporter proteins: MDR3, MRP1,
6 MRP9, MRP2, MRP3, MRP4, NTCP (Sodium-taurocholate cotransporting
7 polypeptide), MCT1 (Monocarboxylate transporter 1), OCTN2 (Organic cation
8 transporter, novel 2), CNT3, ENT1, ENT2 and OATP-H. No genes were classified as
9 poorly expressed and only 11 genes were not expressed at all (MRP6, OCT1/2,
10 OCTN1, OAT1/2/3, CNT1/2, ATB (0+) and OATP-F). Gene expressions were
11 calculated using 18S rRNA as reference gene. Using a single reference gene could
12 represent a limitation of the study, however, 18S rRNA has been indicated as the
13 most suitable reference gene in qPCR normalization of data in the case of other
14 primary human airways epithelial tissues [29].

15 Corticosteroids, which are one of the main topical nasal active ingredients, are an
16 example of a drug class that is associated with these cell transporters [37,38]. In
17 particular, budesonide and beclomethasone dipropionate (BDP) have shown effect
18 of the expression of BCRP, PGP, OCT1 and OCT2 in Calu-3 and breast cancer cell
19 lines [39,40]. In addition, budesonide has been found to be a substrate of P-
20 glycoprotein (ABCB1) in transport experiments across Caco-2 cell line [41].

21 Nevertheless, to our knowledge there is a lack of information about their role in the
22 nose [35]. Our data shows that BCRP and PGP are expressed in the nasal
23 epithelium and in the RPMI 2650 model, suggesting that an avenue for future
24 investigations in this direction.

25

1 Although the xenobiotic genes expression was found to be higher for primary cells
2 than for RPMI 2650 in general, the same genes were expressed in both primary
3 human mucosa nasal cells and RPMI 2650, highlighting the potential use of
4 RPMI2650 grown on ALI as a suitable model for nasal mucosa. In addition, from the
5 47 genes that encode for transporter proteins, the 11 that were not expressed in
6 primary cells were also absent in RPMI 2650, further supporting a good correlation
7 between the RPMI 2650 cell model and human nasal mucosa. The following
8 proteins: NaPi1, URAT1, PEPT1, PEPT2, OATP-C and OATP-8 were found to be
9 expressed in brushed nasal cells, but not in RPMI 2650; this could be considered as
10 a limitation to the RPMI 2650 model in terms of transport of peptides and organic
11 anionic substances.

12

13 Kreft et al. had previously described the expression of some of xenobiotic transporter
14 genes in RPMI 2650 grown in ALI conditions with two different culturing media and at
15 two culturing time points: 1 and 3 weeks, without finding any relevant differences
16 [20]. Our data correlate nicely with those published by Kreft, suggesting good
17 reproducibility of RPMI2650 cell model.

18

19

20 **Development and Validation of the Modified Expansion Chamber**

21 The different materials used for the manufacturing of the FDA guideline expansion
22 chamber (glass) and the 3D printed modified chamber (ABS) could raise the
23 question whether or not the aerosol performances and particle deposition in the two
24 chambers could be different. Therefore, in order to validate the 3D printed modified
25 chamber, the aerosol performance of a commercially available nasal spray

1 (Rhinocort Nasal Spray, AstraZeneca, Australia) was evaluated using a NGI cascade
2 impactor using both expansion chambers. Table 3 shows the percentage of
3 budesonide (calculated as percentage of the emitted nominal dose, 96 µg)
4 recovered in each stage of NGI after 3 actuations of the Rhinocort device (average
5 of 3 runs), using both devices.

6 (Table 3 Here)

7
8 The amount of drugs in the 3D printed modified chamber was calculated as sum of
9 the mass recovered from both the upper and lower hemisphere and the three
10 Snapwells in the chamber. As expected, the majority of the drug was found in the
11 chamber demonstrating that the device produced a coarse spray with an
12 aerodynamic diameter that is higher than 10 µm, with minimal respirable fraction.
13 Overall, there were no statistical differences in aerosol performance for Rhinocort
14 between the modified and the glass chamber for all NGI stages (no drug was
15 recovered for stages lower than 2). With the deposition onto the Snapwell inserts,
16 13.12 ± 0.07 µg of budesonide were recovered from the three cell inserts after the
17 extraction with 80:20 (v/v) methanol/ water, with approximately 4.4 µg of budesonide
18 on each well. This is equivalent to roughly 13.7% of the dose emitted with each
19 spray of the Rhinocort suspension that reaches each Snapwell inserts.

20
21 Having validated the modified chamber in terms of aerosol performance, the RPMI
22 2650 cells grown on Snapwell inserts were introduced into the modified chamber in
23 order to perform cells permeation experiments. The maintenance of barrier
24 properties and the integrity of the cell layers are key factors for permeation studies.
25 In order to confirm that the handling of the Snapwell inserts and the process of

1 deposition into the modified chamber were not hampering the barrier properties of
2 RPMI 2650 nasal cell model, a solution of HBSS was sprayed 6 times on the
3 RPMI2650 nasal cells into the chamber. The cells were removed from the chamber
4 and after 4 hours of Flu-Na permeation studies, the P_{app} was calculated. No
5 statistical differences were found ($p < 0.05$) between the P_{app} values of control and
6 treated cells.

7

8 Finally, deposition and permeation experiments were performed using a budesonide
9 commercial spray and with the 3D printed modified expansion chamber connected to
10 the cascade impactor, using the three Snapwells inserts with RPMI 2650 cells grown
11 for 14 days. The formulation was deposited on the cells after device actuation and
12 RPMI 2650 cells inserts were placed back in cell culture plates to perform the
13 permeation study.

14

15 (Figure 7 Here).

16

17 Figure 7 shows the percentage of budesonide transported across the nasal cell
18 model after deposition in the 3D MC; the In the first hour, approximately 47.3 ± 5.0 %
19 of the drug was transported. This can be explained, as suggested by Baumann, due
20 to the high quantity of available budesonide dissolved in the commercially available
21 product to bind and diffuse readily through the epithelium [42,43]. At the end of the
22 experiment (4 hours), 83.1 ± 6.3 % of the total drug deposited reached the basal
23 compartment. Between three to four hours, a decreased permeation rate was
24 observed, probably due to the depletion of budesonide on the surface of the cells
25 that consequently decreases the gradient between the two compartments (apical

1 and basal). The total amount of budesonide found on each well was on average of
2 $0.79 \pm 0.25 \mu\text{g}$. This was calculated from the sum of the budesonide on, in and
3 transported across the cell layer; **the total amount recovered from each well was**
4 **used as 100% reference value for the calculation in the cell deposition/ transport**
5 **studies.** This variability of the amount of budesonide deposited on each well could be
6 related to both the plume geometry of Rhinocort nasal spray and the manual
7 activation of the device, that don't allow a uniform deposition on each well. The
8 integrity of the cell layer was maintained within the time scaled study with no
9 statistical differences ($p>0.05$) was found between TEER values before (126 ± 21
10 $\Omega\cdot\text{cm}^2$) and after ($127 \pm 14 \Omega\cdot\text{cm}^2$) the transport studies.

11

12 As shown in Figure 8, after 4 hours $14.4 \pm 4.9 \%$ of the drug remains on the surface
13 of the cell and $2.5 \pm 1.6 \%$ of budesonide was found inside the cells, suggesting low
14 binding and internalization within the cells of the RPMI 2650 nasal mucosa model.
15 **This is in good agreement with data published by Baumann showing that lower**
16 **levels of budesonide bind to human nasal tissue when compared with other**
17 **glucocorticoids [42].**

18

19 (Figure 8 Here)

20

21 **CONCLUSION**

22 This research has shown that RPMI 2650 cells could be successfully grown on
23 Snapwell inserts. The cells form a continuous layer offering a permeation barrier
24 similar in terms of trans-epithelial electrical resistance and sodium fluorescein
25 paracellular permeation to previously reported nasal epithelium models and more

1 importantly to excised human nasal mucosa. It was also shown that RPMI 2650 cells
2 produce mucus and its production is related to seeding density and time in culture.
3 The optimal conditions for RPMI 2560 to achieve the highest epithelial barrier and a
4 complete coating with mucus layer are: Snapwell polycarbonate inserts at seeding
5 density of 2.50×10^6 cell/ml and cultured for 14 days in ALI culture. Regarding protein
6 transporters expression, RPMI 2650 cells represent a good model of the nasal
7 epithelium, correlating well with gene expression of freshly collected human nasal
8 epithelial cells. A 3D printed modified expansion chamber, which allow deposition of
9 nasal formulation directly on RPMI 2650 grown on Snapwell inserts has been
10 successfully designed, validated and tested using a commercial nasal spray,
11 showing that this model could be used concomitantly to study nasal formulations
12 aerosol deposition and permeation through a nasal epithelium model of the
13 aerosolized formulation.

14

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19

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21 No conflicts of interest exist.

22

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Table 1. List of drug transporters evaluated and their gene expression (ΔCq) in RPMI2650 cultivated on Snapwells at 2.50×10^6 cell/ml, PNC: human primary nasal cells from brushing (average between male and female). Scale from not expressed (red) to highly expressed (dark green)

Protein Name	Protein Description	Gene code	RPMI 2650	PNC	ΔCq	Classification
P-gp	P-glycoprotein	ABC B1			30	No Expression
BSEP	Bile Salt Export Pump	ABC B11			15 to 30	Poorly Expressed
MDR3	Multidrug resistance protein 3	ABC B4			5 to 15	Expressed
MRP1	Multidrug resistance-associated protein 1	ABC C1			<5	Highly Expressed
MRP7	Multidrug resistance-associated protein 7	ABC C10				
MRP8	Multidrug resistance-associated protein 8	ABC C11				
MRP9	Multidrug resistance-associated protein 9	ABC C12				
MRP2	Multidrug resistance-associated protein 2	ABC C2				
MRP3	Multidrug resistance-associated protein 3	ABC C3				
MRP4	Multidrug resistance-associated protein 4	ABC C4				
MRP5	Multidrug resistance-associated protein	ABC C5				
MRP6	Multidrug resistance-associated protein 6	ABC C6				
BCRP	breast cancer resistance protein	ABC G2				
NTCP	Sodium-taurocholate cotransporting polypeptide	SLC1 0A1				
PEPT1	Peptide transporter 1	SLC1 5A1				
PEPT2	Peptide transporter 2	SLC1 5A2				
MCT1	Monocarboxylate transporter 1	SLC1 6A1				
MCT2	Monocarboxylate transporter 2	SLC1 6A7				
NaPi1	Renal type I sodium/phosphate transporter	SLC1 7A1				
(OCT1)	Organic cation transporter 1	SLC2 2A1				
URAT1	Organic anion/urate transporter 1	SLC2 2A12				
(OCT2)	Organic cation transporter 2	SLC2 2A2				
(OCT3)	Organic cation transporter 3	SLC2 2A3				
OCTN1	Organic cation transporter, novel 1	SLC2 2A4				
OCTN2	Organic cation transporter, novel 2	SLC2 2A5				

OAT1	Organic anion transporter 1		SLC2 2A6		
OAT2	Organic anion transporter 2		SLC2 2A7		
OAT3	Organic anion transporter 3		SLC2 2A8		
CNT1	Anti-Concentrative Transporter 1	Nucleoside	SLC2 8A1		
CNT2	Anti-Concentrative Transporter 2	Nucleoside	SLC2 8A2		
CNT3	Anti-Concentrative Transporter 3	Nucleoside	SLC2 8A3		
ENT1	Equilibrative transporter 1	nucleoside	SLC2 9A1		
ENT2	Equilibrative transporter 2	nucleoside	SLC2 9A2		
ENT3	Equilibrative transporter 3	nucleoside	SLC2 9A3		
ENT4	Equilibrative transporter 4	nucleoside	SLC2 9A4		
OST α	Organic Solute Alpha	Transporter,	SLC5 1A		
ATB(0+)	Sodium- and chloride-dependent neutral and basic amino acid transporter B(0+)		SLC6 A14		
OATP-A	Organic anion polypeptide A	transporter	SLC O1A2		
OATP-C	Organic anion polypeptide C	transporter	SLC O1B1		
OATP-8	Organic anion polypeptide 8	transporter	SLC O1B3		
OATP-F	Organic anion polypeptide F	transporter	SLC O1C1		
PGT	Prostaglandin	Transporter	SLC O2A1		
OATP-B	Organic anion polypeptide B	transporter	SLC O2B1		
OATP-D	Organic anion polypeptide D	transporter	SLC O3A1		
OATP-E	Organic anion polypeptide E	transporter	SLC O4A1		
OATP-H	Organic anion polypeptide H	transporter	SLC O4C1		
OATP-J	Organic anion polypeptide J	transporter	SLC O5A1		

Table 2. P_{app} values ($\times 10^{-6}$ cm/s) of Flu-Na across RPMI 2650 cultured in ALI conditions for three different seeding densities ($n=3$; \pm StDev) compared to values obtained for excised human nasal mucosa

Flu-Na P_{app} values ($\times 10^{-6}$ cm/s)					
Seeding Density	1.25 ($\times 10^6$ cells/ml)	2.50 ($\times 10^6$ cells/ml)	5.00 ($\times 10^6$ cells/ml)	Human Nasal Mucosa	
Freshly excised	-	-	-	3.12 \pm 1.99 [18]	
Week 1	5.32 \pm 0.37	5.21 \pm 0.27	5.47 \pm 0.49		
Week 2	3.67 \pm 0.21	2.68 \pm 0.60	2.95 \pm 0.17		
Week 3	3.47 \pm 0.20	3.55 \pm 0.30	2.69 \pm 0.18		

Table 3. Amount of Budesonide (% of nominal dose) recovered from each Stage of the NGI using the Glass and Modified chamber (n=3 ± StDev).

	Chamber	Connection Tube	Stage 1	Stage 2*
Glass Chamber	98.75±0.09	0.57±0.05	0.50±0.03	0.18±0.04
Modified Chamber	98.73±0.09	0.57±0.07	0.51±0.03	0.19±0.01

* No Budesonide was found below Stage 2

Figure 1. 3D drawing of the modified expansion chamber.

Figure 2. British Pharmacopoeia apparatus E equipped with FDA glass expansion chamber (A) and modified expansion chamber (B).

Figure 3. TEER of three different seeding densities of RPMI2650 cells cultured in the ALI conditions over time (n=3; \pm StDev).

Figure 4. Optical microscope images of Alcian blue mucus staining on RPMI 2650 grown on Snapwell® inserts at 2.50×10^6 cell/ml seeding density.

Figure 5. RGBb ratio values obtained after mucus staining as function of time in culture for the three different cell seeding densities (n=3; \pm StDev).

Figure 6. Confocal Microscope Images of RPMI 2650 cells tight junction proteins-stained in green: E-cadherin (A) and ZO-1 (B-C). The blue and red colours in A and B respectively represent the DAPI staining of nuclei. C, the cross section of cell layers during confocal imaging: green ZO-1 and red cell nucleus.

Figure 7. Amount of budesonide transported through RPMI 2650 nasal cell model after NGI aerosols deposition using the 3D modified chamber (n=5 \pm StDev).

Figure 8. Distribution of the budesonide recovered at the end of the experiment (4 hours) after the aerosol deposition using the 3D the modified expansion chamber ($n=5 \pm StDev$).

Figure 1
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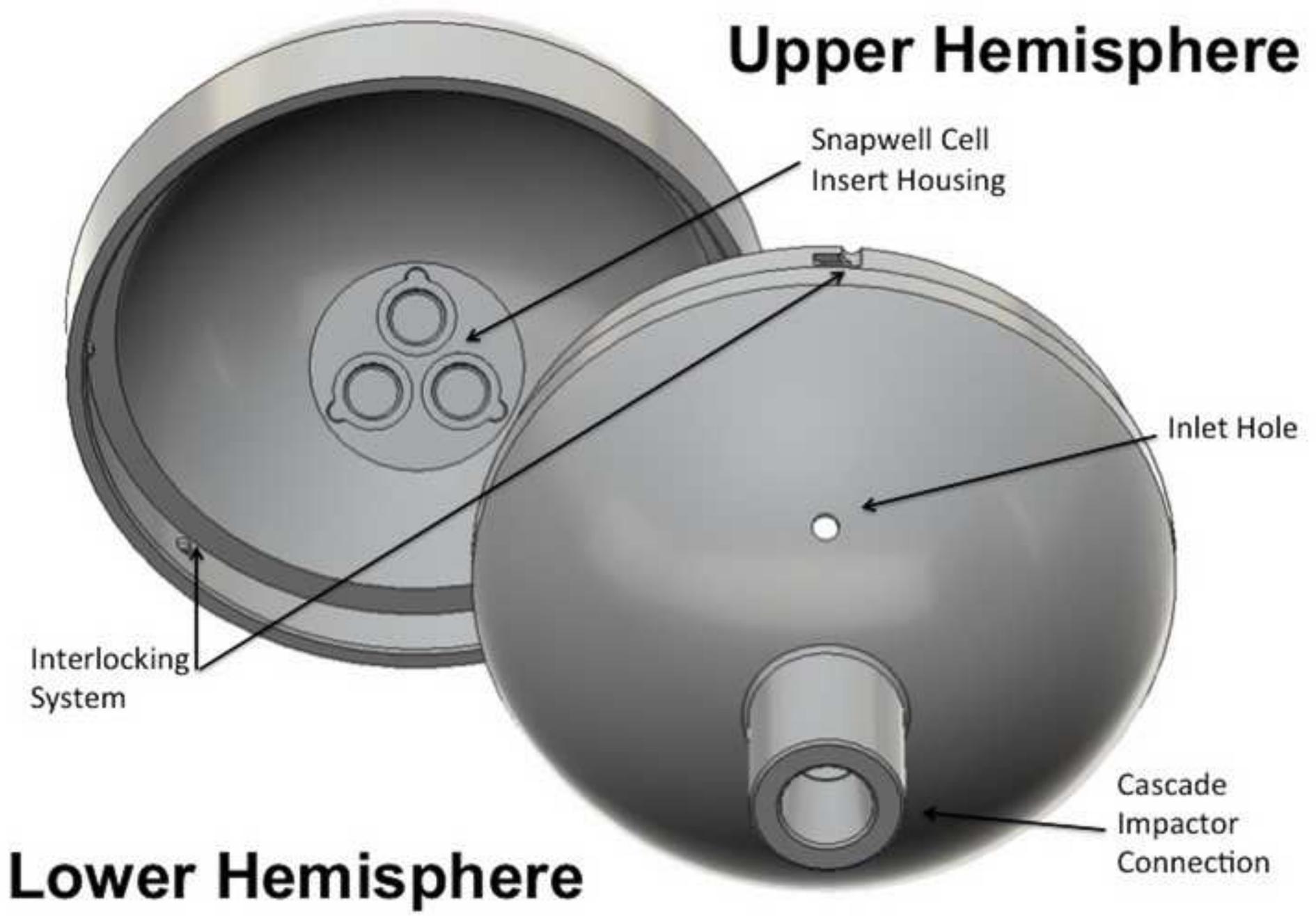


Figure 2
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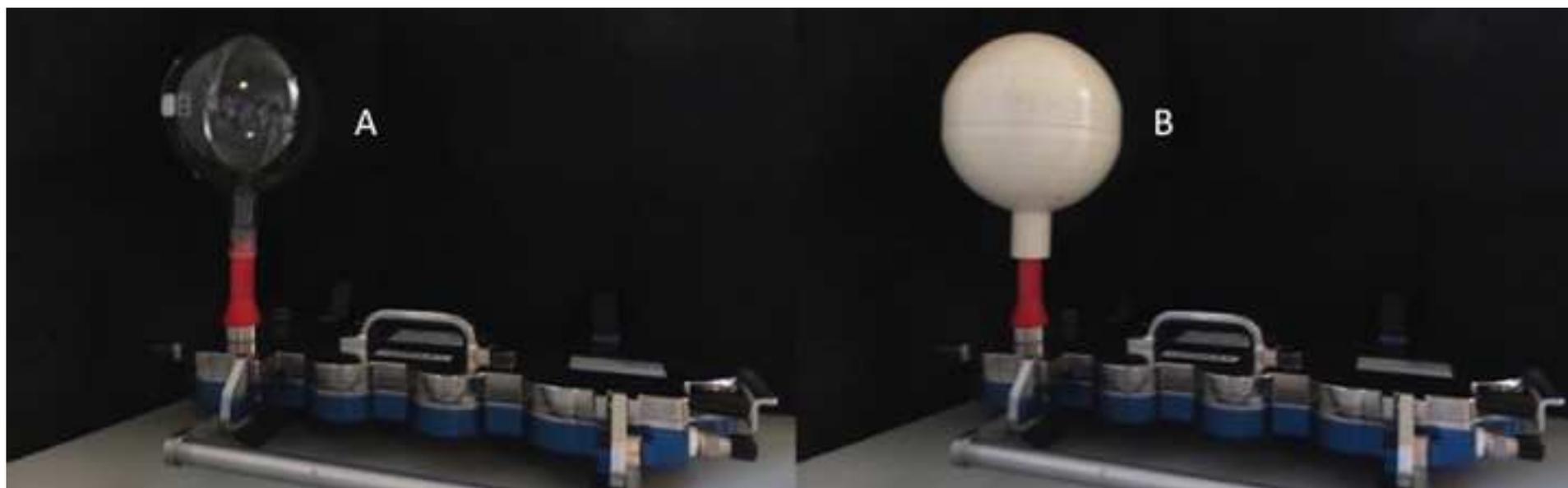


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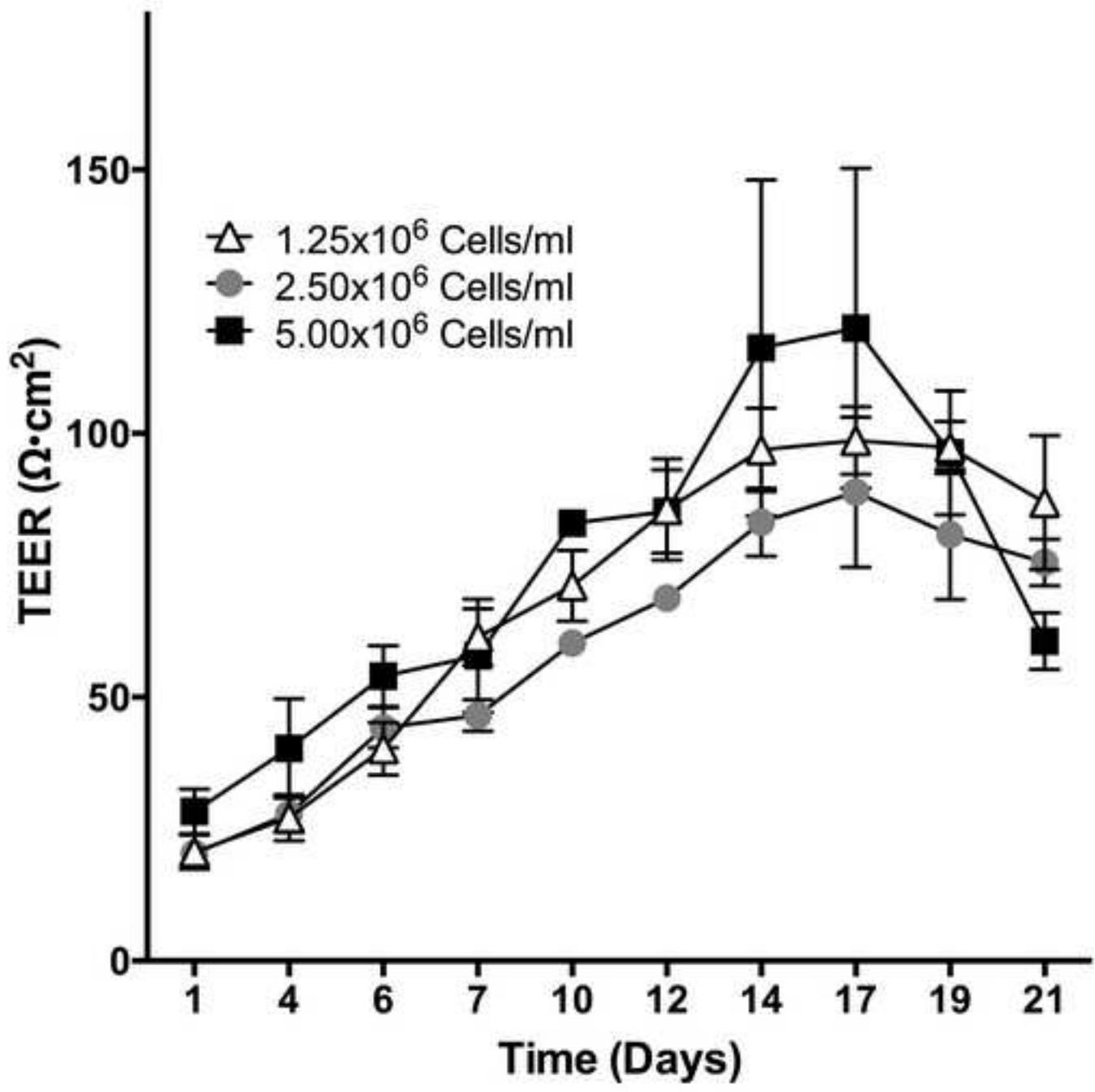


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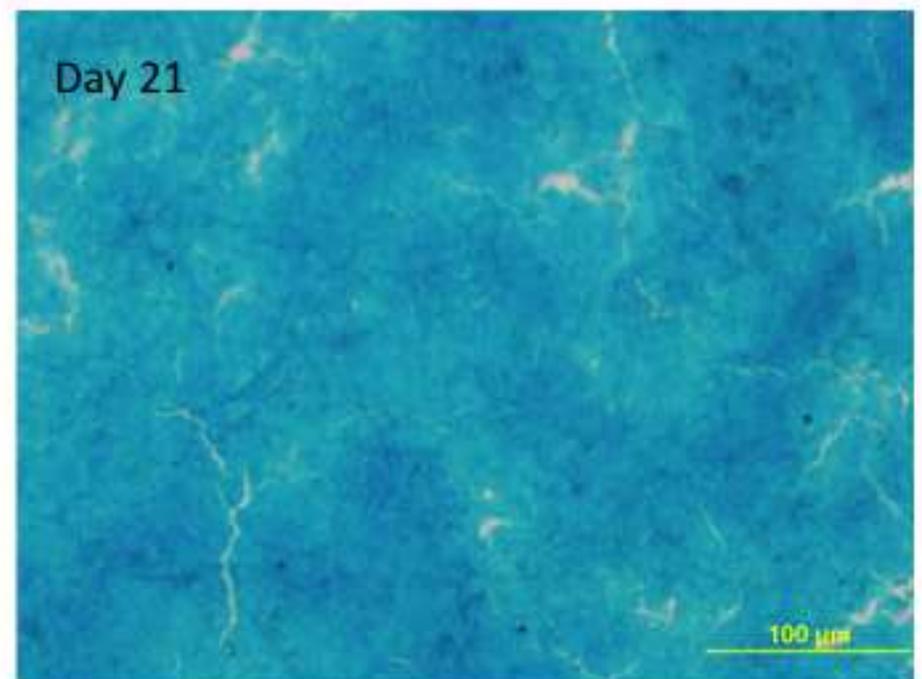
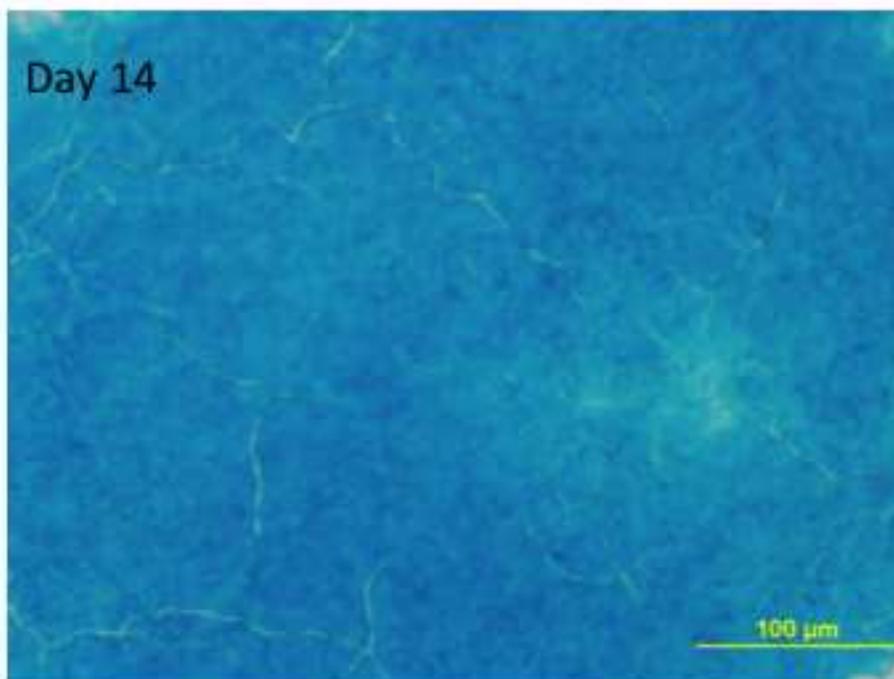
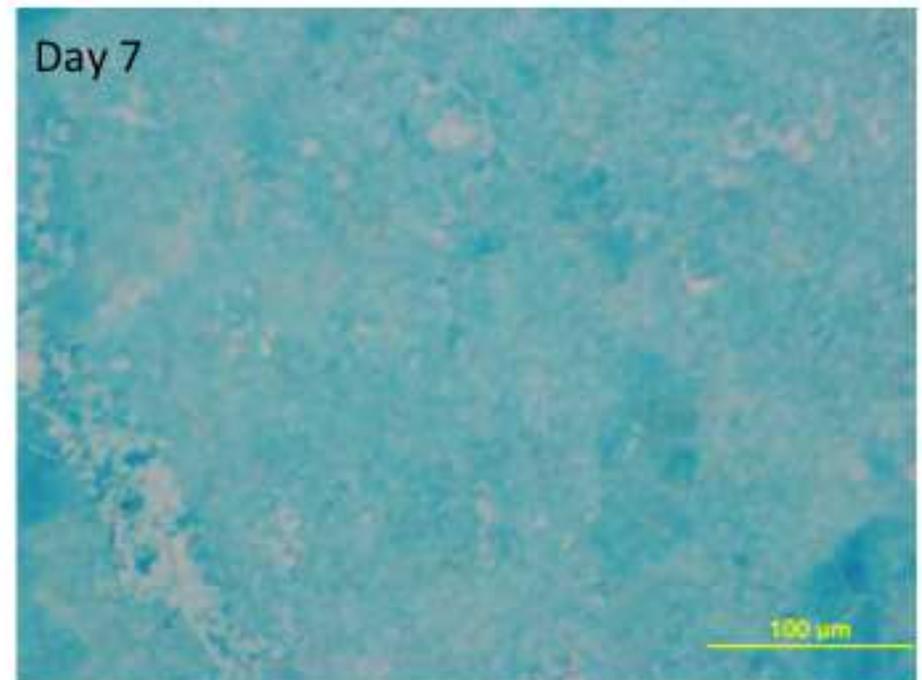
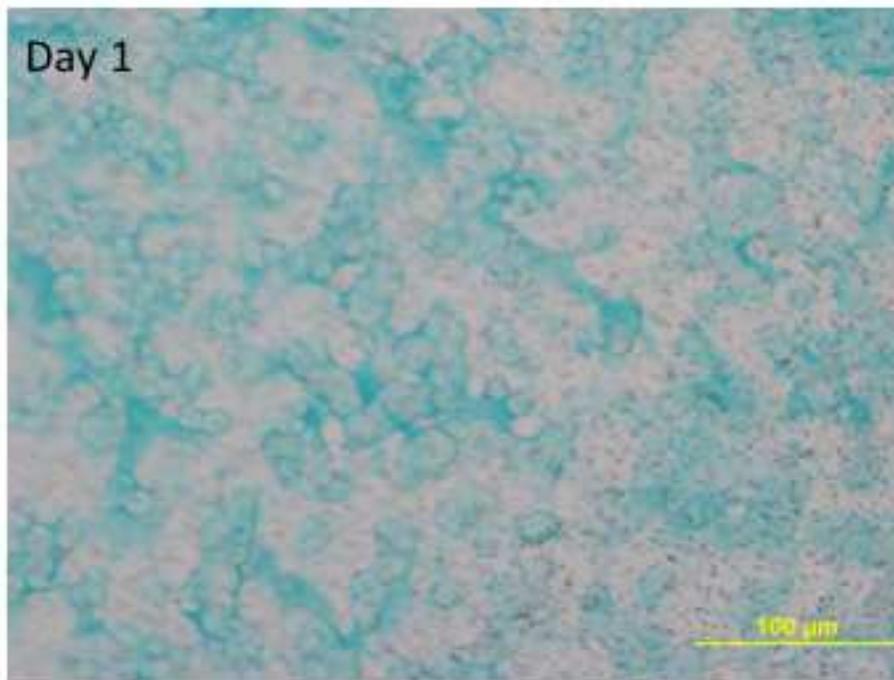


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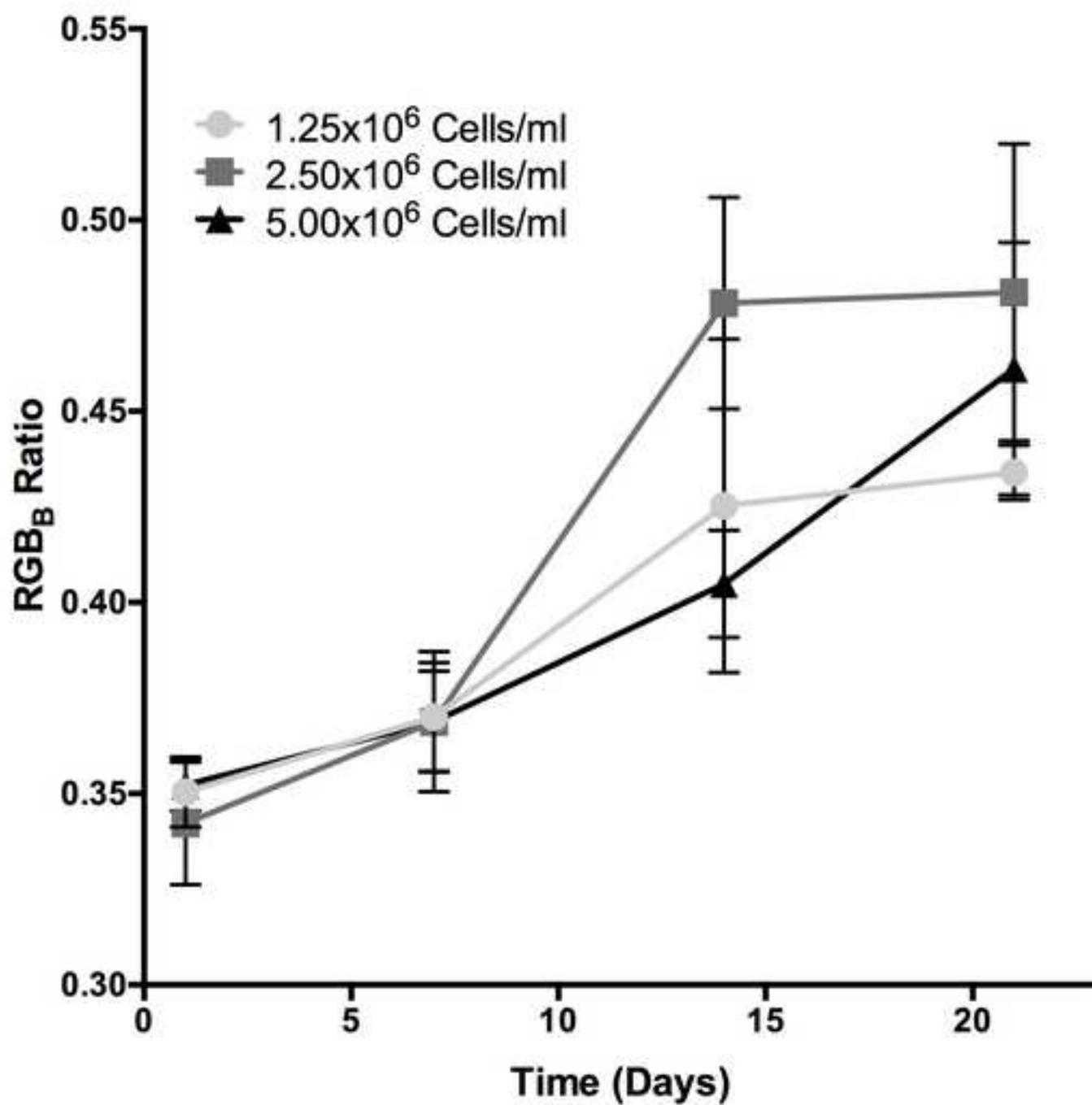


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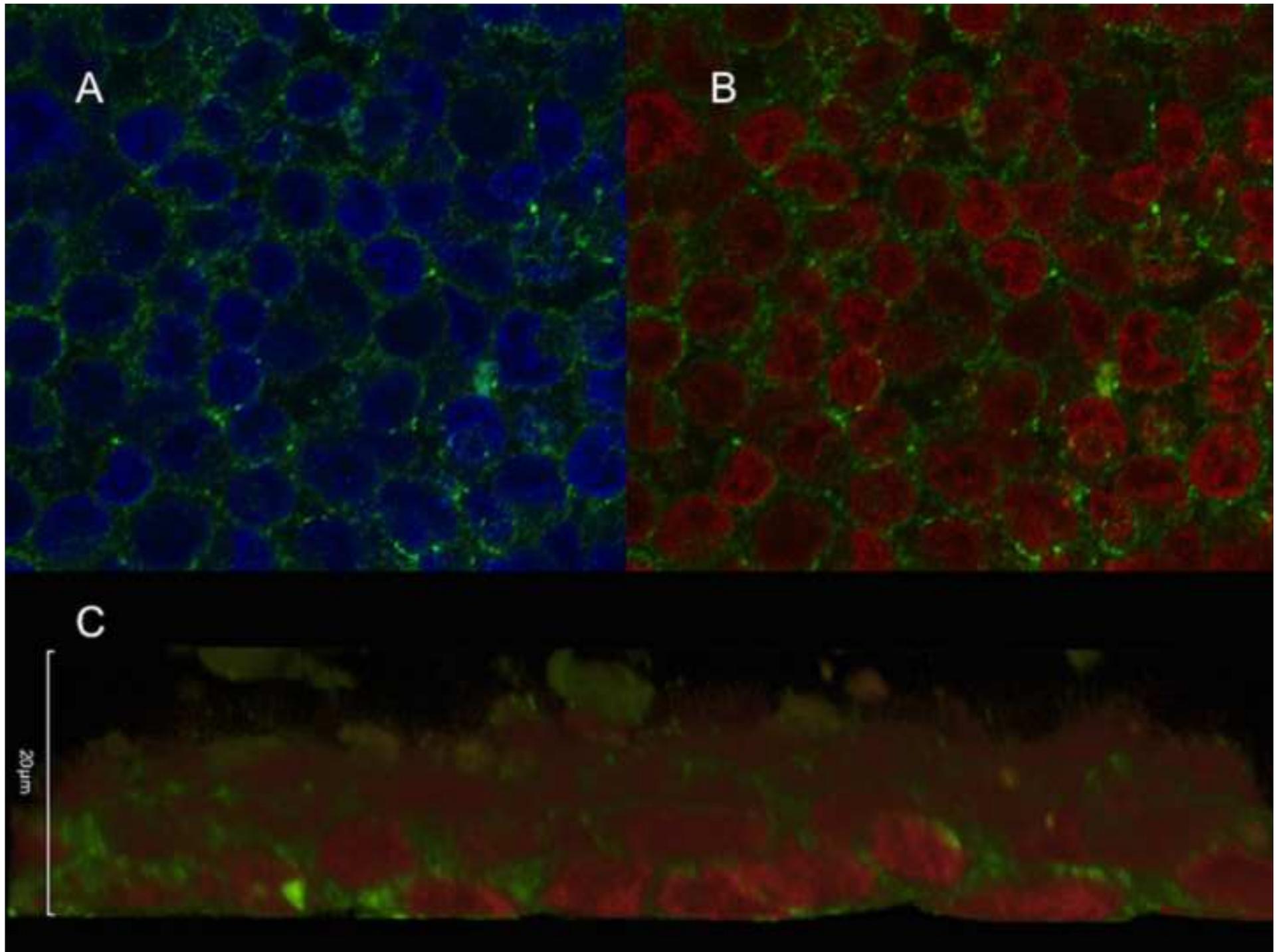


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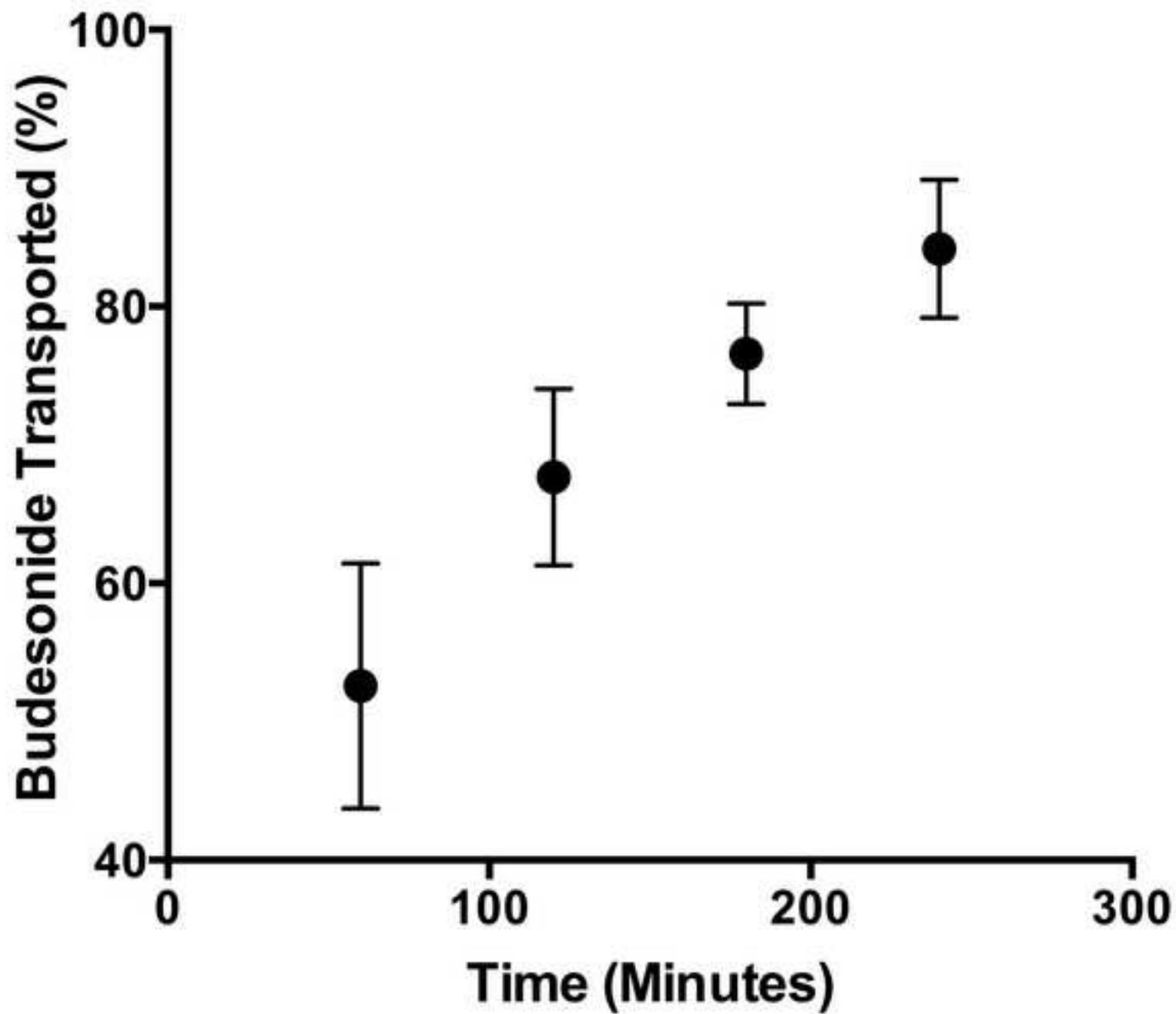


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